



# 1 Functional MRI brain state 2 occupancy in the presence of 3 cerebral small vessel disease – a 4 pre-registered replication analysis of 5 the Hamburg City Health Study

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Preprocessed data is  
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## 20 Abstract

21 **Objective:** To replicate recent findings on the association between the extent of  
22 cerebral small vessel disease (cSVD), functional brain network dedifferentiation, and  
23 cognitive impairment.

24 **Methods:** We analyzed demographic, imaging, and behavioral data from the  
25 prospective population-based Hamburg City Health Study. Using a fully prespecified  
26 analysis pipeline, we estimated discrete brain states from structural and resting-state  
27 functional magnetic resonance imaging (MRI). In a multiverse analysis, we varied brain  
28 parcellations and functional MRI confound regression strategies. The severity of cSVD  
29 was operationalized as the volume of white matter hyperintensities of presumed  
30 vascular origin. Processing speed and executive dysfunction were quantified using the  
31 Trail Making Test (TMT).

32 **Hypotheses:** We hypothesized a) that a greater volume of supratentorial white matter  
33 hyperintensities would be associated with less time spent in functional MRI-derived  
34 brain states of high fractional occupancy; and b) that less time spent in these  
35 high-occupancy brain states is associated with a longer time to completion in part B of  
36 the TMT.

37 **Results:** High-occupancy brain states were characterized by activation or suppression  
38 of the default mode network. Every 5.1-fold increase in WMH volume was associated  
39 with a 0.94-fold reduction in the odds of occupying DMN-related brain states ( $P$   
40  $5.01 \times 10^{-8}$ ). Every 5% increase in time spent in high-occupancy brain states was  
41 associated with a 0.98-fold reduction in the TMT-B completion time ( $P$  0.0116). Findings  
42 were robust across most brain parcellations and confound regression strategies.

43 **Conclusion:** We successfully replicated previous findings on the association between  
44 cSVD, functional brain occupancy, and cognition in an independent sample. The data  
45 provide further evidence for a functional network dedifferentiation hypothesis of  
46 cSVD-related cognitive impairment. Further research is required to elucidate the  
47 mechanisms underlying these associations.

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## 49 Introduction

50 Cerebral small vessel disease (cSVD) is an arteriopathy of the brain associated with age  
51 and common cardiovascular risk factors (Wardlaw, C. Smith, and Dichgans, 2013). cSVD  
52 predisposes patients to ischemic stroke (in particular lacunar stroke) and may lead to  
53 cognitive impairment and dementia (Cannistraro et al., 2019). Neuroimaging findings in  
54 cSVD reflect its underlying pathology (Wardlaw, Valdés Hernández, and Muñoz-Maniega,  
55 2015) and include white matter hyperintensities (WMH), lacunes of presumed vascular

56 origin, small subcortical infarcts and microbleeds, enlarged perivascular spaces as well  
57 as brain atrophy (Wardlaw, E. E. Smith, et al., 2013). However, the extent of visible cSVD  
58 features on magnetic resonance imaging (MRI) is an imperfect predictor of the severity  
59 of clinical sequelae (Das et al., 2019) and our understanding of the causal mechanisms  
60 linking cSVD-associated brain damage to clinical deficits remains limited (Bos et al., 2018).

61 Recent efforts have focused on exploiting network aspects of the structural (Tuladhar,  
62 Dijk, et al., 2016; Tuladhar, Tay, et al., 2020; Lawrence, Zeestraten, et al., 2018) and func-  
63 tional (Dey et al., 2016; Schulz et al., 2021) organization of the brain to understand the  
64 relationship between cSVD and clinical deficits in cognition and other domains that rely  
65 on distributed processing. Reduced structural network efficiency has repeatedly been  
66 described as a causal factor in the development of cognitive impairment, particularly  
67 executive dysfunction and reduced processing speed in cSVD (Lawrence, Chung, et al.,  
68 2014; Shen et al., 2020; Reijmer et al., 2016; Prins et al., 2005). Findings with respect  
69 to functional connectivity (FC), however, are more heterogeneous than their SC counter-  
70 parts, perhaps because FC measurements are prone to be affected by hemodynamic  
71 factors and noise, resulting in relatively low reliability, especially with resting-state scans  
72 of short duration (Laumann, Gordon, et al., 2015). This problem is exacerbated in the  
73 presence of cSVD and worsened by arbitrary processing choices (Lawrence, Tozer, et al.,  
74 2018; Gesierich et al., 2020).

75 As a promising new avenue, time-varying, or dynamic, functional connectivity approaches  
76 have recently been explored in patients with subcortical ischemic vascular disease (Yin  
77 et al., 2022; Xu et al., 2021). Although the study of dynamic FC measures may not solve  
78 the problem of limited reliability, especially in small populations or participants with ex-  
79 tensive structural brain changes, it adds another – temporal – dimension to the study of  
80 functional brain organization, which is otherwise overlooked. Importantly, FC dynamics  
81 not only reflect moment-to-moment fluctuations in cognitive processes, but are also re-  
82 lated to brain plasticity and homeostasis (Laumann and Snyder, 2021; Laumann, Snyder,  
83 et al., 2017), which may be impaired in cSVD.

84 In the present paper, we aimed to replicate and extend the main results of (Schlemm  
85 et al., 2022). In this recent study, the authors analyzed MR imaging and clinical data from  
86 the prospective Hamburg City Health Study (HCHS, (Jagodzinski et al., 2020)) using a coac-  
87 tivation pattern approach to define discrete brain states and found associations between  
88 the WMH load, time spent in high-occupancy brain states characterized by activation or

89 suppression of the default mode network (DMN), and cognitive impairment. Specifically,  
90 every 4.7-fold increase in WMH volume was associated with a 0.95-fold reduction in the  
91 odds of occupying a DMN-related brain state; every 2.5 seconds (i.e., one repetition time)  
92 not spent in one of those states was associated with a 1.06-fold increase in TMT-B com-  
93 pletion times.

94 The fractional occupancy of a functional MRI-derived discrete brain state is a participant-  
95 specific measure of brain dynamics and is defined as the proportion of BOLD volumes  
96 assigned to that state relative to all BOLD volumes acquired during a resting-state scan.

97 Our primary hypothesis for the present work was that the volume of supratentorial  
98 white matter hyperintensities is associated with fractional occupancy of DMN-related  
99 brain states in a middle-aged to elderly population mildly affected by cSVD. Our sec-  
100 ondary hypothesis was that fractional occupancy is associated with executive dysfunc-  
101 tion and reduced processing speed, measured as the time to complete part B of the Trail  
102 Making Test (TMT).

103 Both hypotheses were tested in an independent subsample of the HCHS study popu-  
104 lation using the same imaging protocols, examination procedures, and analysis pipelines  
105 as those in (Schlemm et al., 2022). The robustness of the associations was explored using  
106 a multiverse approach by varying key steps in the analysis pipeline.

## 107 **Methods**

### 108 **Study population**

109 This study analyzed data from the Hamburg City Health Study (HCHS), an ongoing prospec-  
110 tive, population-based cohort study aiming to recruit a cross-sectional sample of 45 000  
111 adult participants from the city of Hamburg, Germany (Jagodzinski et al., 2020). From  
112 the first 10 000 participants of the HCHS, we planned to include those who were docu-  
113 mented to have received brain imaging (n=2648) and exclude those who were analyzed  
114 in our previous report (Schlemm et al., 2022) (n=970). The ethical review board of the  
115 Landesärztekammer Hamburg (State of Hamburg Chamber of Medical Practitioners) ap-  
116 proved the HCHS (PV5131), and all participants provided written informed consent.

### 117 **Demographic and clinical characterization**

118 From the study database, we extracted the participants' age at the time of inclusion in  
119 years, their sex, and the number of years spent in education. During the visit to the study

120 center, participants underwent cognitive assessment using standardized tests. From the  
121 database, we extracted their performance scores on the Trail Making Test part B, mea-  
122 sured in seconds, as an operationalization of executive function and psychomotor pro-  
123 cessing speed (Tombaugh, 2004; Arbuthnott and Frank, 2000). For descriptive purposes,  
124 we also extracted data on past medical history and reported the proportion of partici-  
125 pants with a previous diagnosis of dementia.

## 126 **MRI acquisition and preprocessing**

127 The magnetic resonance imaging protocol for the HCHS includes structural and resting-  
128 state functional sequences. The acquisition parameters for a 3 T Siemens Skyra MRI scan-  
129 ner (Siemens, Erlangen, Germany) have been previously reported (Petersen et al., 2020;  
130 Frey et al., 2021) and are given as follows:

131 For  $T_1$ -weighted anatomical images, a 3D rapid acquisition gradient-echo sequence  
132 (MPRAGE) was used with the following sequence parameters: repetition time  $TR = 2500$  ms,  
133 echo time  $TE = 2.12$  ms, 256 axial slices, slice thickness  $ST = 0.94$  mm, and in-plane resolu-  
134 tion  $IPR = (0.83 \times 0.83)$  mm<sup>2</sup>.

135  $T_2$ -weighted fluid attenuated inversion recovery (FLAIR) images were acquired with  
136 the following sequence parameters:  $TR = 4700$  ms,  $TE = 392$  ms, 192 axial slices,  $ST =$   
137  $0.9$  mm,  $IPR = (0.75 \times 0.75)$  mm<sup>2</sup>.

138 125 resting state functional MRI volumes were acquired ( $TR = 2500$  ms;  $TE = 25$  ms;  
139 flip angle =  $90^\circ$ ; slices = 49;  $ST = 3$  mm; slice gap = 0 mm;  $IPR = (2.66 \times 2.66)$  mm<sup>2</sup>). The  
140 participants were asked to keep their eyes open and to think of nothing.

141 We verified the presence and voxel dimensions of expected MRI data for each par-  
142 ticipant and excluded those for whom at least one of  $T_1$ -weighted, FLAIR, and resting-  
143 state MRI was missing. We also excluded participants with neuroradiologically confirmed  
144 space-occupying intra-axial lesion. To ensure reproducibility, no visual quality assess-  
145 ment of raw images was performed.

146 For the remaining participants, structural and resting-state functional MRI data was  
147 preprocessed using FreeSurfer v6.0 (<https://surfer.nmr.mgh.harvard.edu/>), and fmriPrep  
148 v20.2.6 (Esteban et al., 2019), using default parameters. Participants were excluded if  
149 automated processing using at least one of these packages failed.

## 150 **Quantification of WMH load**

151 For our primary analysis, the extent of ischemic white matter disease was operational-  
152 ized as the total volume of supratentorial WMHs obtained from automated segmentation  
153 using a combination of anatomical priors, BIANCA (Griffanti, Zamboni, et al., 2016), and  
154 LOCATE (Sundaresan et al., 2019), post-processed with a minimum cluster size of 30 vox-  
155 els, as described in (Schlemm et al., 2022). In an exploratory analysis, we partitioned  
156 voxels identified as WMH into deep and periventricular components according to their  
157 distance to the ventricular system (cut-off 10 mm, (Griffanti, Jenkinson, et al., 2018))

## 158 **Brain state estimation**

159 The output from fMRIPrep was post-processed using xcpEngine v1.2.3 to obtain de-confounded  
160 spatially averaged BOLD time series (Ciric, Wolf, et al., 2017). For the primary analysis, we  
161 used the  $36p$  regression strategy and the Schaefer-400 parcellation (Schaefer et al., 2018),  
162 as in (Schlemm et al., 2022).

163 Different atlases and confound regression strategies, as implemented in xcpEngine,  
164 were included in an exploratory multiverse analysis.

165 Co-activation pattern (CAP) analysis was performed by first aggregating parcellated,  
166 de-confounded BOLD signals into a  $(n_{\text{parcels}} \times \sum_i n_{\text{time points},i})$  feature matrix, where  $n_{\text{time points},i}$   
167 denotes the number of retained volumes for participant  $i$  after confound regression.  
168 Clustering was performed using the  $k$ -means algorithm ( $k = 5$ ) with a distance measure  
169 given by 1 minus the sample Pearson correlation between points, as implemented in  
170 Matlab R2021a. We estimated the participant- and state-specific fractional occupancies,  
171 which are defined as the proportion of BOLD volumes assigned to each brain state (Vi-  
172 daurre et al., 2018). The two states with the highest average occupancies were identified  
173 as the basis for further analysis.

## 174 **Statistical analysis**

175 For demographic (age, sex, and years of education) and clinical (TMT-B) variables, the  
176 number of missing items is reported. For non-missing values, we provide descriptive  
177 summary statistics using median and interquartile range. The proportions of men and  
178 women in the sample are reported. Since we expected based on our pilot data (Schlemm  
179 et al., 2022) that the proportion of missing data would be small, primary regression mod-  
180 elling was carried out as a complete-case analysis.

181 As an outcome-neutral quality check of the implementation of the MRI processing  
182 pipeline, brain state estimation, and co-activation pattern analysis, we compared frac-  
183 tional occupancies between brain states. We expected that the average fractional oc-  
184 cupancy in the two high-occupancy states would be higher than the average fractional  
185 occupancy in the other three states. Point estimates and 95% confidence intervals are  
186 presented for the difference in average fractional occupancy to verify this assertion.

187 For further analyses, non-zero WMH volumes were subjected to logarithmic transfor-  
188 mation. Zero values retained their value of zero; to compensate, all models included a  
189 binary indicator for zero WMH volume if at least one non-zero WMH value was present.

190 To assess the primary hypothesis of a negative association between the extent of  
191 ischemic white matter disease and time spent in high-occupancy brain states, we per-  
192 formed a fixed-dispersion Beta regression to model the logit of the conditional expect-  
193 ation of the average fractional occupancy of two high-occupancy states as an affine  
194 function of the logarithmized WMH load. Age and sex were included as covariates. The  
195 strength of the association was quantified as the odds ratio per interquartile ratio of the  
196 WMH burden distribution, and is accompanied by a 95% confidence interval. Significance  
197 testing of the null hypothesis of no association was conducted at the conventional signif-  
198 icance level of 0.05. Estimation and testing were carried out using the 'betareg' package  
199 v3.1.4 in R v4.2.1.

200 To assess the secondary hypothesis of an association between time spent in high-  
201 occupancy brain states and executive dysfunction, we performed a generalized linear  
202 regression with a Gamma response distribution to model the logarithm of the condi-  
203 tional expected completion time in part B of the TMT as an affine function of the average  
204 fractional occupancy of two high-occupancy states. Age, sex, years of education, and  
205 logarithmized WMH load were included as covariates. The strength of the association  
206 was quantified as a multiplicative factor per percentage point and accompanied by a  
207 95% confidence interval. Significance testing of the null hypothesis of no association was  
208 conducted at the conventional significance level of 0.05. Estimation and testing were  
209 performed using the glm function included in the 'stats' package from R v4.2.1.

## 210 **Pre-registered analyses**

211 The analysis plan was pre-registered on June 27 2023 at <https://osf.io/fcqmb>. The sample  
212 size calculation was based on an effect size on the odds ratio scale of 0.95, correspond-  
213 ing to an absolute difference in the probability of occupying a DMN-related brain state

214 between the first and third WMH-load quartile of 1.3 percentage points, and between  
215 the 5% and 95% percentile of 3.1 percentage points. Approximating half the difference  
216 in fractional occupancy of DMN-related states between different task demands (rest vs  
217 n-back) in healthy participants, which was estimated to lie between 6 and 7 percentage  
218 points (Cornblath et al., 2020), this value represented a plausible choice for the smallest  
219 effect size of theoretical and practical interest. It also equals the estimated effect size  
220 based on the data presented in (Schlemm et al., 2022).

221 Simple bootstrapping was used to create 10 000 hypothetical datasets of size 200, 400,  
222 600, 800, 900, 910, ..., 1090, 1100, 1200, 1400, 1500, and 1600. Each dataset was then sub-  
223 jected to the estimation procedure described above. For each sample size, the propor-  
224 tion of datasets in which the primary null hypothesis of no association between fractional  
225 occupancy and WMH load could be rejected at  $\alpha = 0.05$  was computed and recorded as  
226 a power curve in Figure 1.

227 A sample size of 960 would have allowed the replication of the reported effect with a  
228 power of 80.2%. We had anticipated a sample size of 1500, which would have yielded a  
229 power of 93.9%.

## 230 **Multiverse analysis**

231 In both (Schlemm et al., 2022) and our primary replication analysis, we made certain ana-  
232 lytical choices in the operationalization of brain states and ischemic white matter disease,  
233 namely the use of the  $36p$  confound regression strategy, the Schaefer-400 parcellation,  
234 and a BIANCA/LOCATE-based WMH segmentation algorithm. The robustness of the as-  
235 sociation between WMH burden and time spent in high-occupancy states with regard to  
236 other choices was explored in a multiverse analysis (Steege et al., 2016). Specifically, in  
237 an exploratory analysis, we estimated brain states from BOLD time series processed ac-  
238 cording to a variety of established confound regression strategies and aggregated over  
239 different cortical brain parcellations (Table 1, Ciric, Rosen, et al., 2018; Ciric, Wolf, et al.,  
240 2017). The extent of cSVD was additionally quantified by the volume of deep and periven-  
241 tricular white matter hyperintensities.

242 For each combination of analytical choice of confound regression strategy, parcella-  
243 tion, and subdivision of white matter lesion load ( $9 \times 9 \times 3 = 243$  scenarios in total), we  
244 quantified the association between WMH load and average time spent in high-occupancy  
245 brain states using odds ratios and 95% confidence intervals as described above.

246 No hypothesis testing was performed for these multiverse analyses. Rather, they

247 serve to inform about the robustness of the outcome of the test of the primary hypoth-  
248 esis. Any substantial conclusions about the association between the severity of cerebral  
249 small vessel pathology and the time spent in high-occupancy brain states were drawn  
250 from the primary analysis using pre-specified methodological choices, as stated in the  
251 Scientific Question in Table 0.

## 252 **Further exploratory analysis**

253 In previous work, two high-occupancy brain states have been related to the default mode  
254 network (Cornblath et al., 2020). We further explored this relationship by computing, for  
255 each individual brain state, the cosine similarity of the positive and negative activations of  
256 the cluster's centroid with a set of a priori defined functional 'communities' or networks  
257 (Schaefer et al., 2018; Yeo et al., 2011). The results were visualized as spider plots for the  
258 Schaefer atlases.

259 In further exploratory analyses, we describe the associations between brain state dy-  
260 namics and other measures of cognitive ability such as memory and language.

## 261 **Pilot data and analysis**

262 Summary data from the first 1000 imaging data points of the HCHS have been published  
263 with (Schlemm et al., 2022) and formed the basis for the hypotheses tested in this replica-  
264 tion study. Before pre-registration, we had implemented our prespecified analysis pipeline  
265 described above in R and Matlab, and applied it to this previous sample. Data, code  
266 and results from this pilot analysis have been stored with the archived Stage 1 report on  
267 GitHub ([https://github.com/csi-hamburg/HCHS\\_brain\\_states\\_RR](https://github.com/csi-hamburg/HCHS_brain_states_RR), v1.5) and preserved on  
268 Zenodo.

## 269 **Timeline and access to data**

270 At the time of planning of this study, all demographic, clinical and imaging data used in  
271 this analysis had been collected by the HCHS and were held in the central trial database.  
272 Quality checks for non-imaging variables had been performed centrally. WMH segmen-  
273 tation based on structural MRI data of the first 10 000 participants of the HCHS had been  
274 performed previously using the BIANCA/LOCATE approach (Rimmele et al., 2022). Func-  
275 tional MRI data and clinical measures of executive dysfunction (TMT-B scores) had not  
276 previously been analyzed by the pre-registering author (ES).

## 277 **Deviations from preregistration**

278 For deconfounding and aggregating BOLD data at brain parcellation level, the software  
279 xcpEngine was used in version 1.2.3, not 1.2.1, to ensure that that the correct MNI ref-  
280 erence template (MNI152Nlin2009cAsym) is used for registration of brain atlases. This  
281 decision was made before analysing the data.

## 282 **Results**

283 For this replication study, a total of 2648 datasets were available, of which 970 were al-  
284 ready included in our previous analysis and thus discarded. In 13 of the resulting 1678  
285 datasets, one or more MRI sequences were missing. Of the complete datasets (n=1665),  
286 we excluded 5 participants due to intra-axial space-occupying lesions. An additional 9  
287 participants were excluded because of unsuccessful preprocessing, WMH segmentation,  
288 or xcpEngine failure, resulting in 1651 datasets for analysis. A study-flowchart is provided  
289 in Figure 2.

290 Baseline demographic and cognitive values, including the number of missing items,  
291 are reported in Table 3.

292 WMH volumes (median 1.05 mL, IQR 0.47 mL to 2.37 mL), motion estimates, and frac-  
293 tional occupancies of brain states 1 through 5 are reported in Table 5.

294 In an outcome-neutral quality check of the implementation of (i) the MRI processing  
295 pipeline, (ii) brain state estimation, and (iii) co-activation pattern analysis, the mean differ-  
296 ence in fractional occupancy between high- and low-occupancy states was consistently  
297 maintained, with a point-estimate of the separation between two high-occupancy and  
298 three low-occupancy states of 6.7% (95% confidence interval, 6.2% to 7.1%) in the 36p  
299 paradigm. This indicates that the implementation of the pipeline was correct and that  
300 the brain state estimation and co-activation pattern analysis worked as intended.

## 301 **Pre-registered hypotheses**

### 302 Association between WMH load and fractional occupancy

303 The results of the test of our primary preregistered hypothesis of an association be-  
304 tween supratentorial WMH volume and the time spent in high-occupancy brain states  
305 are shown in Figure 3 and Table 7.

306 Adjusted for age and sex, there was a 0.94-fold reduction in the odds of occupying a  
307 high-occupancy brain state for every 5.1-fold increase in WMH load ( $P 5.01 \times 10^{-8}$ ).

308 Association between executive function and fractional occupancy in DMN-  
309 related states

310 The results of the test of our secondary preregistered hypothesis of an association be-  
311 tween time spent in high-occupancy brain states and executive function as measured by  
312 the complete part B of the TMT are shown in Figure 4 and Table 9.

313 Adjusted for age, sex, WMH volume, and years of education, there was a 0.98-fold  
314 reduction in the time to complete the TMT-B for every 5 % increase in the time spent in  
315 high-occupancy brain states (P 0.0116).

### 316 **Multiverse analysis**

317 In a multiverse analysis, the main findings of associations between WMH load and FO  
318 and, to a lesser extent, between FO and TMT-B were robust with respect to the processing  
319 choices of brain parcellation and confound regression strategy.

320 A nominally statistically significant negative association between the total WMH load  
321 and time spent in high-occupancy states was observed in 48/81 scenarios, with 8/81 sig-  
322 nificant positive associations occurring with the Desikan–Killiany parcellation only (Fig-  
323 ure 5A). For periventricular (deep) WMH volume, the results were similarly robust with  
324 49/81 (39/81) negative and 8/81 (0/81) positive associations of nominal statistical signifi-  
325 cance, respectively.

326 The secondary finding of an association between greater TMT-B times and lower frac-  
327 tional occupancy was less robust with only 16/81 nominally statistically significant neg-  
328 ative and no significant positive associations, irrespective of operationalization of cSVD  
329 (total vs. periventricular vs. deep WMH volume) (Figure 5B).

### 330 **Additional analyses**

331 Connectivity profiles of brain states – relation to default mode network  
332 Based on the cosine similarity between positive and negative activations of cluster cen-  
333 troids and indicator vectors of pre-defined large scale brain networks, network activation  
334 profiles were computed for brain states estimated from Schaefer parcellations of varying  
335 spatial resolutions.

336 Figure 6 shows the corresponding spider plots, identifying states characterized by  
337 activation (DMN+) or suppression (DMN-) of the default mode network as states with the  
338 highest fractional occupancy.

### 339 Association with other cognitive domains

340 Associations between the time spent in high-occupancy DMN-related brain states and  
341 cognitive measures beyond TMT-B are shown in Figure 7.

342 Adjusted for age, sex, WMH load, and years of education, FO in DMN-related states  
343 appeared to be associated with better word recall (adjusted OR 1.19, nominal P 0.013),  
344 but not with global cognitive functioning (MMSE, adjusted OR 1.09) or vocabulary (aOR  
345 1.09), nor with verbal fluency (animal naming, adjusted  $\exp(\beta)$  1.04), or pure processing  
346 speed (TMT-A, adjusted  $\exp(\beta)$  0.97).

## 347 Summary and Discussion

348 In this pre-registered cross-sectional study we replicated the key findings of Schlemm  
349 et al., 2022 in an independent population-based sample of 1651 middle-aged to elderly  
350 participants of the Hamburg City Health Study.

351 First, we confirmed that the severity of cerebral small vessel disease is associated with  
352 the time spent in high-occupancy brain states, defined by functional MRI. More precisely,  
353 we showed that every 5.1-fold increase in the volume of supratentorial white matter hy-  
354 perintensities of presumed vascular origin (WMH) was associated with a 0.95-fold reduc-  
355 tion in the odds of occupying a brain state characterized by activation or suppression of  
356 the default-mode network, at any given time during the resting-state scan.

357 Second, we confirmed that the time spent in high-occupancy brain states at rest is  
358 associated with cognitive performance. More precisely, a 5%-reduction in the fractional  
359 occupancy of DMN-related brain states was associated with a 1.02-fold increase in the  
360 time to complete part B of the trail making test (TMT).

361 In a pre-planned multiverse analysis, findings relating to our primary and, to a lesser  
362 extent, secondary hypotheses were robust with respect to variations in brain parcel-  
363 lations and confound regression strategies. Inconsistent results were found with the  
364 Desikan–Killiany parcellation, likely reflecting the notion that the spatial resolution and  
365 functional specificity of this coarse, structurally defined atlas are inadequate for analyz-  
366 ing functionally defined brain states. Across brain parcellations, effect sizes were smaller  
367 with the ICA-AROMA confound regression strategy and failed to reach nominal statisti-  
368 cal significance. This might be due to a relatively large residual motion component in  
369 measures of dynamical functional Connectivity after de-noising with ICA-AROMA, as de-  
370 scribed previously (Lydon-Staley et al., 2019).

371 We also confirmed across several brain parcellation resolutions that high-occupancy  
372 states at rest are characterized by either activation or suppression of the default mode  
373 network, reflecting its role as the predominant task-negative brain network.

374 In unplanned, exploratory analyses, we described the association between brain state  
375 dynamics and cognitive measures other than executive function and processing speed  
376 and reported a strong, preliminary association between time spent in high-occupancy  
377 states and delayed word recall.

378 We further explored, and report in the Supplementary appendix, the effect of mo-  
379 tion; results relating to our primary and, to a lesser extent, secondary, hypotheses were  
380 robust to additional, unplanned adjustments for DVARS, RMSD, and mean framewise  
381 displacement.

382 The presented results provide robust evidence for a behaviorally relevant association  
383 between cerebral small vessel disease and functional brain network dedifferentiation.

384 Further research is required to replicate our findings in different populations, such  
385 as those affected more severely by cSVD or cognitive impairment, or being studied using  
386 different imaging protocols, to determine the generalizability of our findings with respect  
387 to varying operationalizations of the notions of cSVD, brain state, and cognition, and to  
388 understand the mechanisms underlying the reported associations.

## 389 **Acknowledgment**

390 This preprint was created using the LaPreprint template ([https://github.com/roaldarbol/](https://github.com/roaldarbol/lapreprint)  
391 [lapreprint](https://github.com/roaldarbol/lapreprint)) by Mikkel Roald-Arbøl .

## 392 **Disclosure**

393 The authors of this article declare that they have no financial conflict of interest with the  
394 content of this article.

## 395 **References**

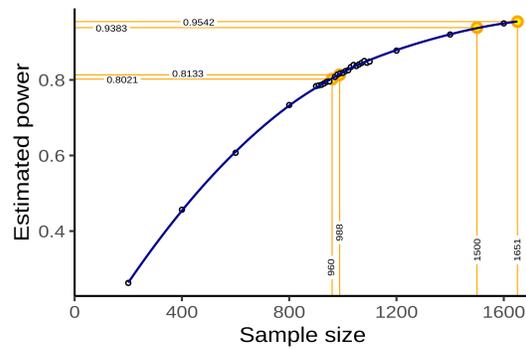
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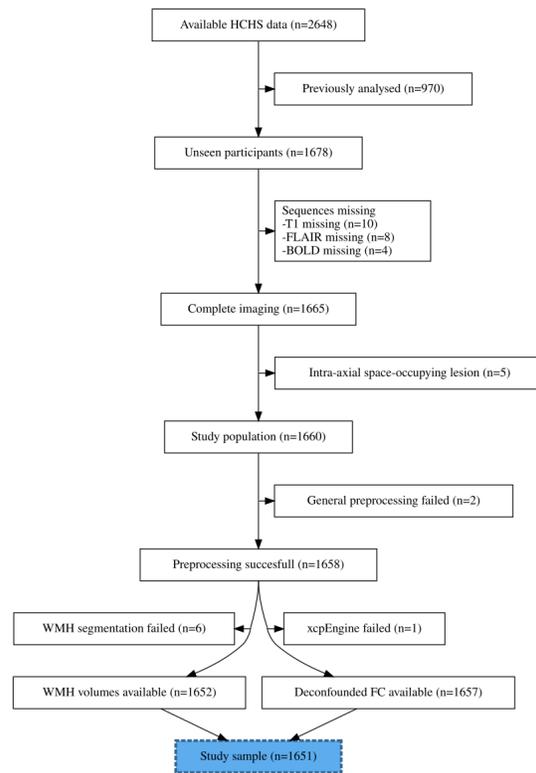
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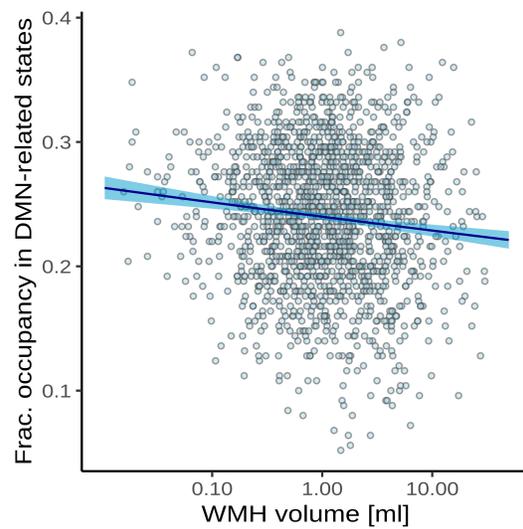
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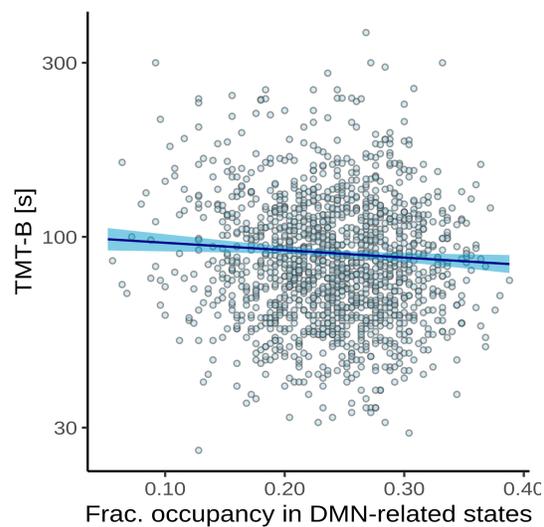
**Figure 1 | Sample size and power estimation.** A-priori estimated power for different sample sizes was obtained as the proportion of synthetic data sets in which the null hypothesis of no association between WMH volume and time spent in high-occupancy brain states can be rejected at the  $\alpha = 0.05$  significance level. Proportions are based on a total of 10 000 synthetic data sets obtained by bootstrapping the data presented in (Schlemm et al., 2022). Highlighted in orange are the smallest sample size ensuring a power of at least 80 % ( $n = 960$ ), the sample size of the pilot data ( $n = 988$ , post-hoc power 81.3 %), the expected sample size for this replication study ( $n = 1500$ , a-priori power 93.9 %), and the achieved sample size ( $n = 1651$ , a-priori power 95.4 %).



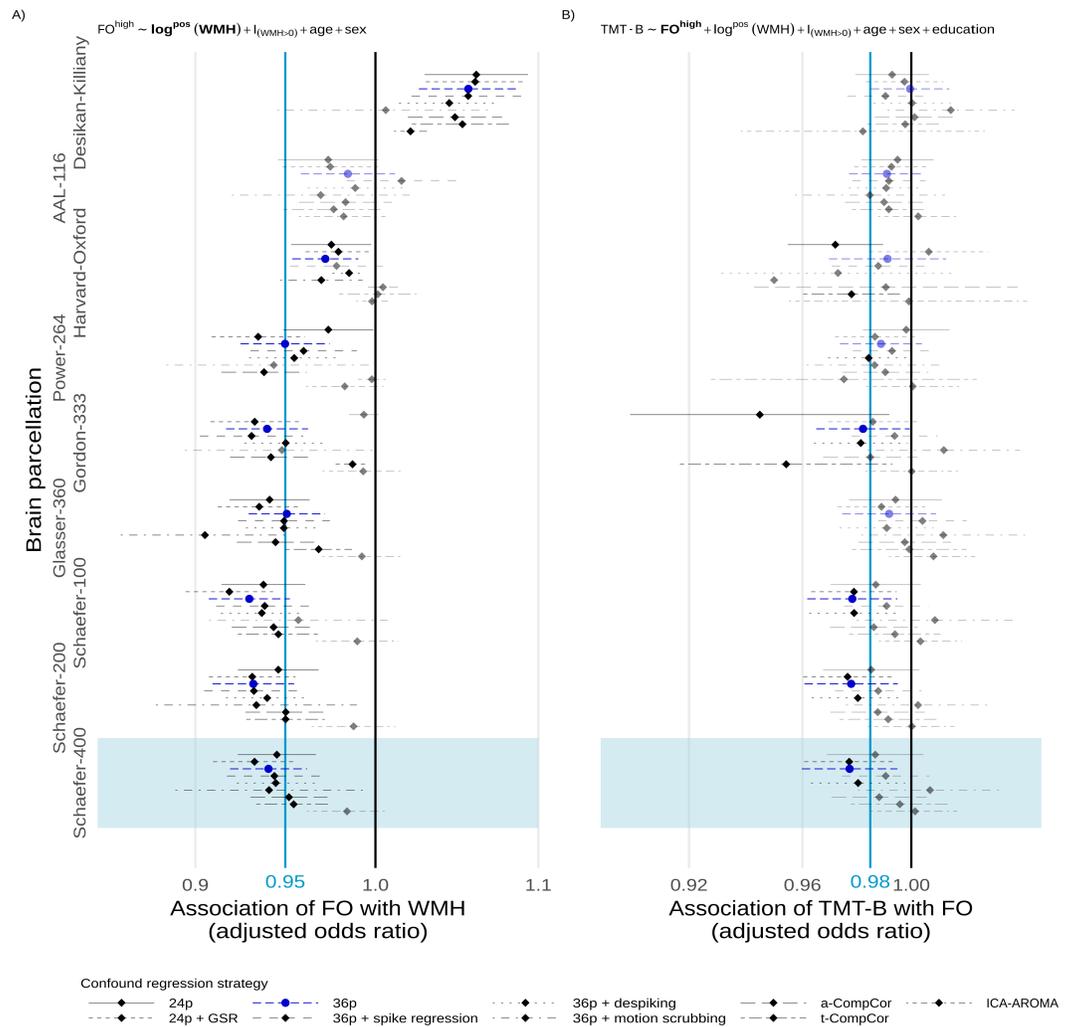
**Figure 2 | Study flowchart.** Composition of the study population after application of inclusion and exclusion criteria, and image processing.



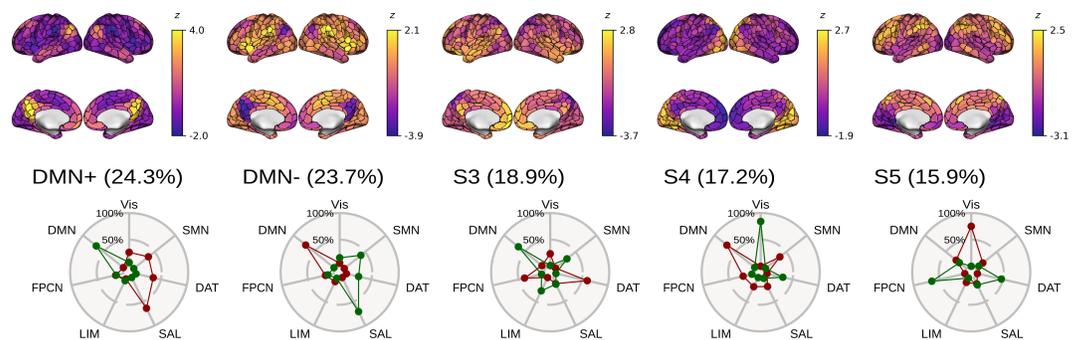
**Figure 3 | Association between time spent in high-occupancy brain states and supratentorial WMH volume.** Point estimates (black line) and 95%-confidence region (light blue ribbon) of the conditional mean fractional occupancy are obtained from unadjusted beta regression modelling. Each marker represents one of N=1642 independent participants with a non-zero total WMH volume.



**Figure 4 | Association between time spent in high-occupancy DMN-related brain states and TMT-B completion time.** Point estimates (black line) and 95%-confidence region (light blue ribbon) of the conditional mean TMT-B completion time are obtained from unadjusted Gamma regression modelling. Each marker represent one of N=1482 independent participants with non-zero total WMH volume and available TMT-B data.

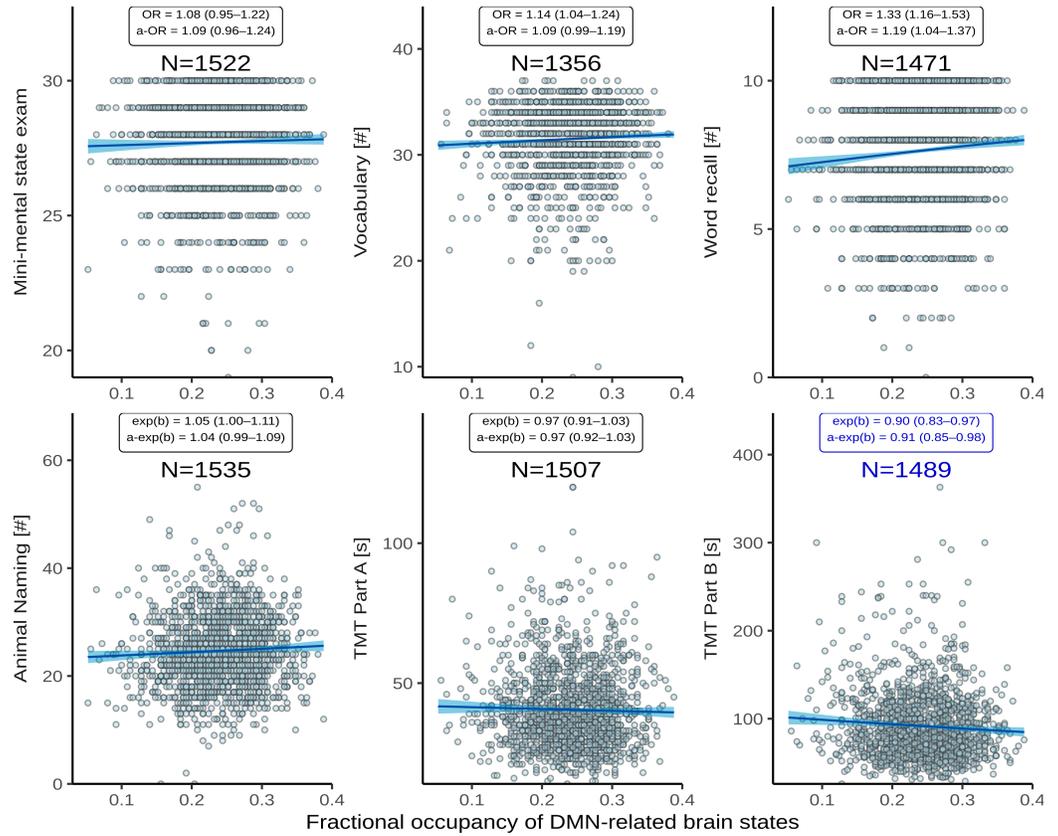


**Figure 5 | Multiverse analysis.** Adjusted effect size estimates of the associations between cSVD severity (WMH volume) and network dedifferentiation (less time spent in high-occupancy DMN-related brain states) [A], and between network dedifferentiation and executive function (TMT-B completion time) [B]. Effect sizes are given per 5.1-fold increase in WMH volume and a 5%-increase in fractional occupancy, respectively. Markers and line segments indicate point estimates and 95%-confidence intervals for adjusted odds ratios for different combinations of confound regression strategy and brain parcellation. The primary analytical choices are indicated by dark blue circles (36p) and light blue shading (Schaefer-400). Model equations for beta and gamma regressions, respectively, are given at the top. Vertical lines indicate no effect (black) and the effect size observed in the discovery cohort (Schlemm et al., 2022) (light blue), respectively, for reference. Effect sizes not reaching nominal statistical significance ( $\alpha = 0.05$ ) are shown desaturated. Corresponding data based on periventricular and deep WMH volumes are presented in the Supplementary Appendix.



**Figure 6 | Connectivity profiles of brain states.** [Top] Centroids of each identified brain state visualized in brain space. Note the individual color scales. [Bottom] Cosine similarity between centroids of brain states and signed indicator vectors corresponding to activation (green) and suppression (red) of each of seven predefined large-scale functional brain networks (Yeo et al., 2011).

States are ordered by mean fractional occupancy across  $N=1651$  independent participants, indicated by parenthetical percentages. Two high-occupancy states are characterized by activation or suppression of the DMN, the remaining three low-occupancy states (S3–5) were not used in the present study. Note that mean FO values are similar, but not identical, to median FO values reported in Table 5.



**Figure 7 | Association between time spent in high-occupancy DMN-related brain states and cognitive measures.** Point estimates (black line) and 95%-confidence region (light blue ribbon) of the conditional mean cognitive measures are obtained from unadjusted binomial (top row: Mini-Mental State Examination, Vocabulary, Word List Recall, logit link) and Gamma regression (bottom row: Animal Naming, Trail Making Test [TMT] A/B: log link) modelling. Each marker represents one of N independent participants, as indicated. Insets report effect sizes and P-values both with (adjusted [a-]) and without adjustment for the nuisance variables age, sex, WMH volume (coded as in Figure 5), and years of education. Effect sizes were quantified as odds ratios (ORs) (top) or response scale multipliers [exp(b)] (bottom), and correspond to a 20%-increase in fractional occupancy. Note the different reference change in FO compared to Table 9 chosen to adequately represent some of the smaller effect sizes. The bottom right panel highlighted in dark blue reproduces Figure 4.

Question	Hypothesis	Sampling plan	Analysis plan	Rationale for deciding the sensitivity of the test	Interpretation given different outcomes	Theory that could be shown wrong by the outcome
Is severity of cerebral small disease, quantified by the volume of supratentorial white matter hyperintensities of presumed vascular origin (WMH), associated with time spent in high-occupancy brain states, defined by resting-state functional MRI?	<b>(Primary)</b> Higher WMH volume is associated with lower average occupancy of the two highest-occupancy brain states.	Available participants with clinical and imaging data from the the HCHS (Jagodzinski et al., 2020)	Standardized preprocessing of structural and functional MRI data • automatic quantification of WMH • co-activation pattern analysis • multivariable generalised regression analyses	Tradition	$P < 0.05 \rightarrow$ rejection of the null hypothesis of no association between cSVD and fractional occupancy; $P > 0.05 \rightarrow$ insufficient evidence to reject the null hypothesis	Functional brain dynamics are not related to subcortical ischemic vascular disease.
Is time spent in high-occupancy brain states associated with cognitive impairment, measured as the time to complete part B of the trail making test (TMT)?	<b>(Secondary)</b> Lower average occupancy of the two highest-occupancy brain states is associated with longer TMT-B time.	as above	as above	as above	$P < 0.05 \rightarrow$ rejection of the null hypothesis of no association between fractional occupancy and cognitive impairment; $P > 0.05 \rightarrow$ insufficient evidence to reject the null hypothesis	Cognitive function is not related to MRI-derived functional brain dynamics.

**Table 0 | Study Design Template.** Overview of the Scientific Questions addressed in the present study (first column), the two main hypotheses being investigated (second column), and details of the underlying study.

Name of the atlas	#parcels	Reference
Desikan–Killiany	86	Desikan et al., 2006
AAL	116	Tzourio-Mazoyer et al., 2002
Harvard–Oxford	112	Makris et al., 2006
glasser360	360	Glasser et al., 2016
gordon333	333	Gordon et al., 2016
power264	264	Power, Cohen, et al., 2011
schaefer{N}	100	Schaefer et al., 2018
	200	
	400	

AAL: Automatic Anatomical Labelling

(a) Parcellations

Design	Reference
24p	Friston et al., 1996
24p + GSR	Macey et al., 2004
36p	Satterthwaite et al., 2013
36p + spike regression	Cox, 1996
36p + despiking	Satterthwaite et al., 2013
36p + scrubbing	Power, Mitra, et al., 2014
aCompCor	Muschelli et al., 2014
tCompCor	Behzadi et al., 2007
AROMA	Pruim et al., 2015

GSR: Global signal regression, AROMA: Automatic Removal of Motion Artifacts

(b) Confound regression strategies, adapted from (Circi, Wolf, et al., 2017)

**Table 1 | Multiverse analysis.** Overview over different brain parcellations and confound regression strategies implemented using xcpEngine (Circi, Rosen, et al., 2018). A total of  $9 \times 9 = 81$  analytical combinations were explored to assess the robustness of our results with respect to these processing choices.

<b>N = 1,651</b>	
<i>Demographics (no Missing n (%))</i>	
Age, yr	
Median (IQR)	66 (59 – 72)
Sex	
Male	940/1651 (57%)
Female	711/1651 (43%)
<i>Cardiovascular risk factors</i>	
Hypertension	
Present	1177/1611 (73.1%)
Missing n (%)	85 (5.1%)
Diabetes	
Present	157/1566 (10%)
Missing n (%)	40 (2.4%)
Smoking	
Present	200/1360 (14.7%)
Missing n (%)	201 (12.9%%)
Hyperlipidaemia	
Present	426/1578 (27%)
Missing n (%)	73 (4.4%)
<i>Cognitive test results</i>	
MMSE, # (max. 30)	
Median (IQR)	28 (27 – 29)
Missing n (%)	129 (7.8%)
Vocabulary (MWT-B), # (max. 37)	
Median (IQR)	32 (30 – 34)
Missing n (%)	295 (18%)
Word recall, # (max. 10)	
Median (IQR)	8 (6 – 9)
Missing n (%)	180 (11%)
Animal Naming	
Median (IQR)	24 (20 – 29)
Missing n (%)	116 (7.0%)
TMT-A, seconds	
Median (IQR)	38 (31 – 48)
Missing n (%)	144 (8.7%)
TMT-B, seconds	
Median (IQR)	83 (65 – 110)
Missing n (%)	162 (9.8%)
<i>History</i>	
Diagnosed dementia	
Present	6/1645 (0.4%)
Missing n (%)	6 (0.4%)
Years of education	
Median (IQR)	13 (12 – 16)
Missing n (%)	34 (2%)

**Table 3 | Descriptive statistics of the study population.** Data are presented as median (interquartile range) or count (percentage) of non-missing items, as appropriate. Number of percentage of missing items are reported separately.

<b>N = 1,651</b>	
WMH volume <sup>1</sup> , mL	
Total	1.05 (0.47 – 2.37), 9 Z
Periventricular	0.94 (0.43 – 2.04), 9 Z
Deep	0.10 (0.03 – 0.37), 344 Z
Motion during rs-fMRI	
Frame-wise displacement, mm	0.21 (0.15 – 0.63)
RMSD, mm	0.086 (0.058 – 0.12)
DVARs	27.8 (24.3 – 31.8)
Fractional occupancy, %	
DMN+	24.8 (20.8 – 28.0)
DMN-	24.0 (20.0 – 28.0)
S3	18.4 (15.2 – 22.4)
S4	16.8 (12.8 – 20.8)
S5	15.2 (12.0 – 19.2)

<sup>1</sup>Number of zero values indicated by Z

**Table 5 | Structural and functional imaging characteristics.** Data are presented as median (interquartile range). Supratentorial WMH volumes were obtained by semiautomatic segmentation of FLAIR images using a BINACA/LOCATE-based *k*-nearest neighbours algorithm and stratified by their distance to the lateral ventricles (<10 mm, periventricular; >10 mm, deep). Motion parameters were estimated during fMRIprep processing of BOLD scans. Fractional occupancies were calculated by assigning individual BOLD volumes to one of five discrete brain states defined by *k*-means clustering-based co-activation pattern analysis. Two high-occupancy states are labelled DMN+ and DMN- in view of their network connectivity profiles as shown in Figure 6.

	Estimate	P	95%-CI
Intercept	0.24	<0.0001	0.21 – 0.27
WMH, per 5.1-fold increase <sup>1</sup>	0.94	<0.0001	0.92 – 0.96
Age, per 10 years	1.04	0.001	1.01 – 1.06
Female sex	1.12	<0.0001	1.09 – 1.16
$\mathbf{1}_{\{\text{WMH}=0\}}$	0.93	0.477	0.75 – 1.14

<sup>1</sup> Interquartile ratio  $2.37/0.468 = 5.06$

**Table 7 | Association between time-spent in high-occupancy DMN-related brain states and WMH volume adjusted for age and sex.** Beta regression table estimated from  $n = 1651$  independent participants using the model equation  $\text{FO}^{\text{high}} \sim \log \text{WMH}^+ + \mathbf{1}_{\{\text{WMH}=0\}} + \text{age} + \text{sex}$ .

	Estimate	P	95%-CI
Intercept	53.41	< 0.0001	42.7 – 66.8
FO <sup>high</sup> , per 5%	0.98	0.0116	0.96 – 0.99
WMH, per 5.1-fold increase <sup>1</sup>	1.01	0.367	0.98 – 1.05
Age, per 10 years	1.18	<0.0001	1.15 – 1.21
Female sex	0.99	0.666	0.95 – 1.03
Education, per year	0.97	<0.0001	0.97 – 0.98
$\mathbf{1}_{\{\text{WMH}=0\}}$	0.97	0.398	0.92 – 1.03

<sup>1</sup> Interquartile ratio 2.37/0.468 = 5.06

**Table 9 | Association between TMT-B and time spent in high-occupancy DMN-related brain states adjusted for age, sex, WMH volume and years of education.** Gamma regression table

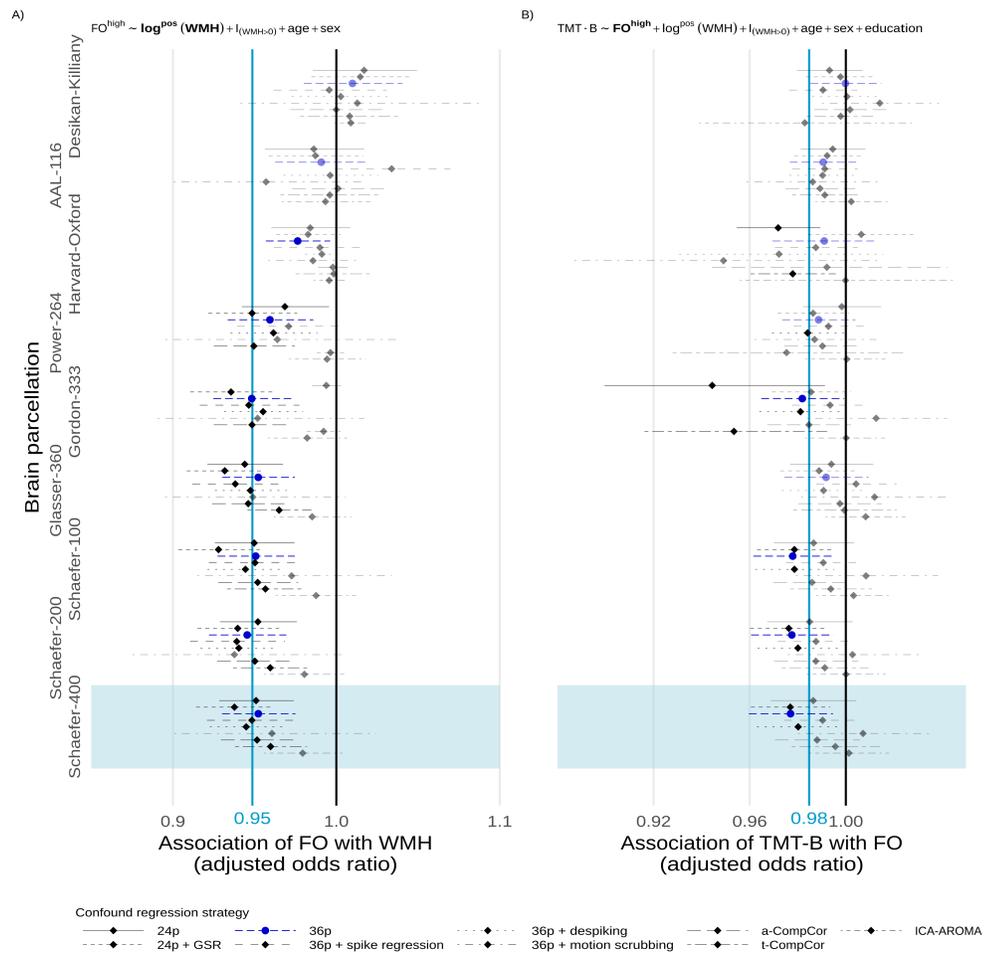
estimated from  $n = 1483$  independent participants using the model equation

$\text{TMT-B} \sim \text{FO}^{\text{high}} + \log \text{WMH}^+ + \mathbf{1}_{\{\text{WMH}=0\}} + \text{age} + \text{sex} + \text{educationyears}$ .

533 **Supplementary results**

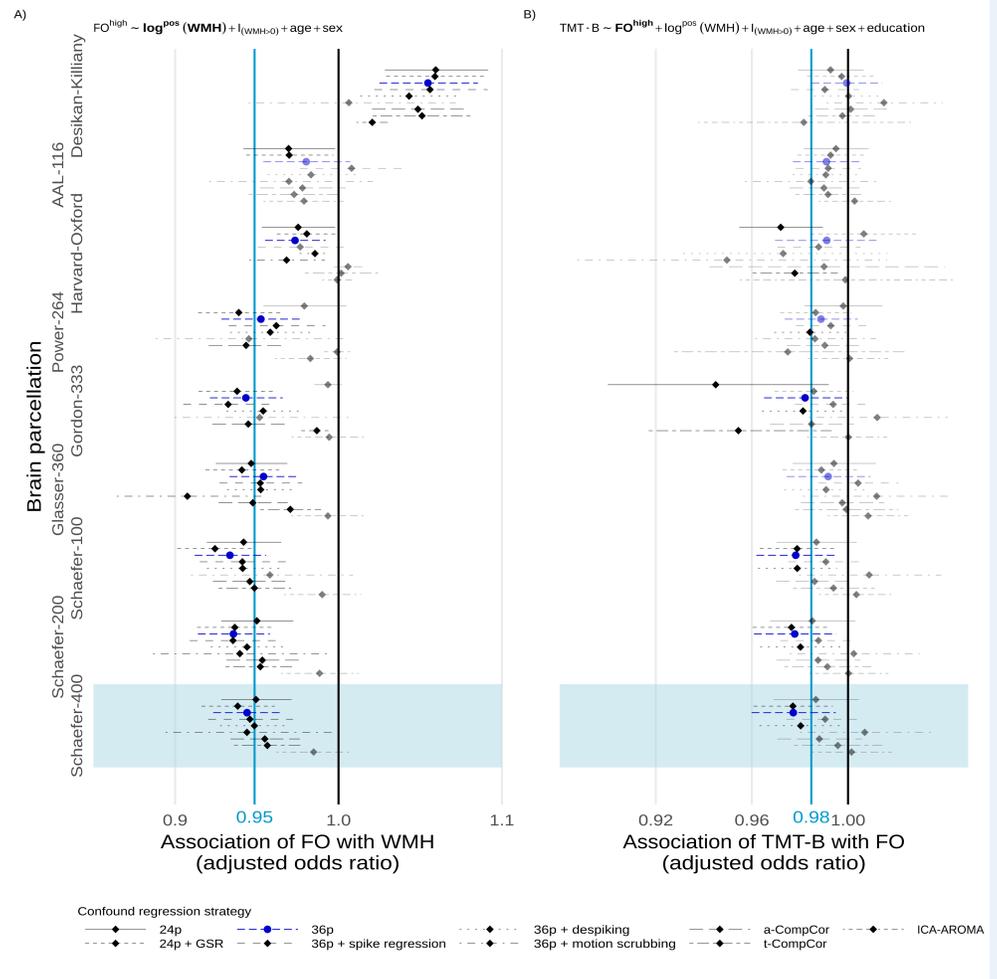
534 **Deep and periventricular WMH**

535 Here we present, in analogy to Figure 5, the results of the multiverse analyses of  
 536 the association between cSVD burden, FO of DMN-related states, and executive  
 537 function, when cSVD is operationalized as the volume of deep or periventricular  
 538 white matter hyperintensities, respectively.



539 **Appendix 1—figure 1 Multiverse analysis, deep WMH**

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543

## Appendix 1—figure 2 Multiverse analysis, periventricular WMH

545

### Motion parameters

546

We also present, in analogy to Tables 7 and 9, regression tables for the association between time spent in DMN-related brain states (FO) and WMH volume, and between TMT-B and FO, adjusted for DVARS, RSMD and framewise displacement, in addition to age, sex and, in the latter case, years of education.

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	Estimate	P	95%-CI
Intercept	0.32	<0.0001	0.28 – 0.36
WMH, per 5.1-fold increase <sup>1</sup>	0.96	0.0004	0.94 – 0.98
Age, per 10 years	1.01	<0.0001	1.00 – 1.01
Female sex	1.11	<0.0001	1.08 – 1.15
$\mathbb{1}_{\{WMH=0\}}$	0.91	0.3552	0.74 – 1.11

DVARs	0.98	<0.0001	0.98 – 0.99
RMSD	28.29	0.0055	2.67 – 299.84
Frame-wise displacement	0.16	0.0112	0.04 – 0.66

<sup>1</sup> Interquartile ratio 2.37/0.468 = 5.06

**Appendix 1—table 2** Association between time-spent in high-occupancy DMN-related brain states and WMH volume adjusted for age, sex, and **motion parameters**

	Estimate	P	95%-CI
Intercept	46.83	<0.0001	36.74 – 59.72
FO <sup>high</sup> , per 5%	0.71	0.0718	0.49 – 1.03
WMH, per 5.1-fold increase <sup>1</sup>	1.01	0.3414	0.98 – 1.04
Age, per 10 years	1.02	<0.0001	1.01 – 1.02
Female sex	1.00	0.8171	0.96 – 1.04
Education, per year	0.97	<0.0001	0.97 – 0.98
$1_{\{WMH=0\}}$	0.96	0.7581	0.73 – 1.29
DVARs	1.01	0.0001	1.00 – 1.01
RMSD	0.31	0.4695	0.01 – 7.45
Frame-wise displacement	1.08	0.9322	0.16 – 7.13

<sup>1</sup> Interquartile ratio 2.37/0.468 = 5.06

**Appendix 1—table 4** Association between TMT-B and time spent in high-occupancy DMN-related brain states adjusted for age, sex, WMH volume and years of education, and **motion parameters**